Effect of robotic gait training on cardiorespiratory system in incomplete spinal cord injury

Femke Hoekstra, MSc;1–3* Michiel P. M. van Nunen, PhD;1–2 Karin H. L. Gerrits, PhD;2 Janneke M. Stolwijk-Swüste, MD, PhD;1 Martine H. P. Crins, MSc;1 Thomas W. J. Janssen, PhD1–2
1Amsterdam Rehabilitation Research Center | Reade, Amsterdam, the Netherlands; 2Faculty of Human Movement Sciences, MOVE Research Institute Amsterdam, VU University Amsterdam, Amsterdam, the Netherlands; 3Center for Human Movement Sciences, University of Groningen, University Medical Center Groningen, Groningen, the Netherlands

Abstract—The objectives in this study were to investigate the effect of robot-assisted gait training on cardiorespiratory fitness in subjects with motor incomplete spinal cord injury and document the exercise intensity of robotic walking in comparison with the recommended guidelines. Ten patients followed a 24-session training program with a robotic gait orthosis in addition to physiotherapy sessions completed within 10 to 16 wk. Cardiorespiratory fitness was determined in a graded arm crank exercise test before and after the training program. To assess the intensity of robot-assisted walking, oxygen consumption (VO2) and heart rate (HR) were measured during a training session early in and at the end of the training program, and exercise intensity measures (percentage of VO2 reserve [%VO2R], percentage of HR reserve [%HRR], and metabolic equivalents [METs]) were calculated. Whereas no changes were found in peak VO2, the resting and submaximal HR at a constant work load were significantly lower after training. Most subjects exercised at low intensity (<30%VO2R, <30%HRR, <3.0 METs), and only two subjects exercised at moderate intensity (>3.0 METs). In spite of the low exercise intensity of the training program and no changes in peak VO2, robot-assisted gait training induced some improvement in cardiorespiratory fitness, as suggested by lower resting and submaximal HR values.

Key words: aerobic training, cardiorespiratory fitness, exercise, exercise intensity, heart rate, locomotor training, oxygen consumption, rehabilitation therapy, robot-assisted gait training, robotic walking, spinal cord injury.

INTRODUCTION

Physical inactivity is commonly reported in the population with spinal cord injury (SCI) [1] and is a major risk factor for developing cardiovascular disease (CVD) [2–3]. Being physically active reduces the risk of CVD and a

Abbreviations: %HRR = percentage of heart rate reserve, %VO2R = percentage of oxygen consumption reserve, ACSM = American College of Sports Medicine, AIS = American Spinal Injury Association Impairment Scale, BWS = body-weight support, CVD = cardiovascular disease, ECG = electrocardiogram, FES = functional electrical stimulation, GF = guidance force, HR = heart rate, iSCI = incomplete spinal cord injury, MET = metabolic equivalent, SCI = spinal cord injury, VO2 = oxygen consumption.

*Address all correspondence to Femke Hoekstra, MSc; Center for Human Movement Sciences, University of Groningen, University Medical Center Groningen, Antonius Deusinglaan 1, Sector F, Rm 3216-0219, 9713 AV Groningen, the Netherlands; 31-50-363-6185.
Email: f.hoekstra@umcg.nl
http://dx.doi.org/10.1682/JRRD.2012.10.0186

Clinical Trial Registration: ISRCTN Register, ISRCTN67827069, “Recovery of Walking Ability Using a Robotic Device”; http://www.controlled-trials.com/ISRCTN67827069
wide range of other medical conditions such as diabetes and obesity [4–6]. Therefore, interventions to promote physical activity in the population with SCI are becoming increasingly important. Traditional exercise modes to improve physical fitness for the population with SCI are arm exercise in a wheelchair or using an arm ergometer and leg exercise with functional electrical stimulation (FES). However, the prevalence of shoulder pain, mostly as a result of overuse, is very high in wheelchair users [7–9]. Therefore, an exercise modality without the repetitive use of upper limbs may be preferable. Through use of FES exercise, the large muscles of the legs can be activated, which can lead to a wide range of fitness and health benefits [10–11]. However, about half of the population with SCI have incomplete lesions, which makes the application of FES painful for many of these individuals [12]. As an alternative, robot-assisted gait training with the Lokomat (Hocoma AG, Volketswil, Switzerland) was introduced as a form of aerobic exercise for these individuals with incomplete SCI (iSCI) [13].

The Lokomat is a device consisting of two robotic arms and a treadmill with a body-weight support (BWS) system. The robotic arms can be attached to the patient’s legs and the body weight is supported by a BWS system while walking on the treadmill [14–15]. Speed, BWS, and amount of assistance can be adjusted to individual ability in order to create a challenging environment where patients can practice stepping. Most studies investigating robot-assisted gait training in iSCI focused on the effectiveness of improving neurologic and motor function and concluded that it is an appropriate therapy for improving walking ability [16–17]. Although there is some knowledge with regard to the cardiovascular effects of BWS treadmill training with manual assistance [13,18–21], little is documented about the cardiorespiratory effects of robot-assisted gait training.

Promising results with regard to cardiovascular effects of robot-assisted therapy have been reported in the population with SCI [22–25]. A recent cross-sectional study by Jack et al. showed that, with vigorous active participation of patients, a substantial increase in heart rate (HR) and oxygen consumption (\(\dot{V}O_2\)) can be achieved [24]. However, without the voluntary activity of the patient (i.e., passive walking) exercise intensity (HR and \(\dot{V}O_2\)) was much lower and probably insufficient to stress the cardiopulmonary system according to the levels of intensity for aerobic training recommended by the American College of Sports Medicine (ACSM). Recently, through use of more sophisticated controllers of the orthoses, gait patterns during robotic walking are less prescribed, and more variation in the gait pattern is possible. These new controllers allow active participation of patients in the kinematics of locomotion, which may be more effective for motor learning [26–27]. However, the effects on the cardiorespiratory system have not yet been studied. Furthermore, little has been documented about longitudinal changes in cardiopulmonary fitness by Lokomat therapy in patients with SCI [13]. Therefore, this study had two goals. The primary purpose of this study was to investigate the effect of a period of active robot-assisted gait training on cardiopulmonary fitness in subjects with a motor iSCI. The secondary purpose of the study was to document the exercise intensity of robotic walking in comparison with the guidelines recommended by the ACSM for exercise intensity.

METHODS

Subjects

Ten subjects with a motor iSCI participated in this study (Table 1). The inclusion criteria were paraplegia or tetraplegia as a result of a motor iSCI (American Spinal Injury Association Impairment Scale [AIS] levels C and D [28]), minimum age of 18 yr, height between 150 and 195 cm, and maximum body mass of 115 kg. The limitations to height and body mass were necessary because of the design of the Lokomat device. The exclusion criteria were medical complications such as uncontrolled cardiac dysrhythmia and other unstable cardiovascular problems, severe skeletal problems such as osteoarthritis or recent fractures of the lower limbs, severe cognitive and/or communicative disorders, other neurological and/or psychiatric disorders, severe spasticity, open wounds or unhealed skin, thrombosis, pneumonia, or other problems that make it impossible to properly accomplish the tasks. Information about the type and location of the lesion was obtained through a clinical evaluation by a physician. After a detailed explanation of the purpose and the protocol of the experiments, all subjects signed an informed consent. The study was approved by the ethics committee of the VU University Medical Center Amsterdam.

Study Design

A single-group pretest-posttest design was used to investigate whether cardiorespiratory fitness improved
Table 1. Subject characteristics at baseline.

<table>
<thead>
<tr>
<th>Subject</th>
<th>Sex</th>
<th>Age (yr)</th>
<th>Height (cm)</th>
<th>Body Mass (kg)</th>
<th>Lesion Level</th>
<th>Time Postinjury (yr)</th>
<th>AIS Level</th>
<th>LEMS</th>
</tr>
</thead>
<tbody>
<tr>
<td>C1</td>
<td>M</td>
<td>52</td>
<td>185</td>
<td>79</td>
<td>L1–L2</td>
<td>9</td>
<td>C</td>
<td>11</td>
</tr>
<tr>
<td>C2</td>
<td>F</td>
<td>31</td>
<td>161</td>
<td>50</td>
<td>T9–T10</td>
<td>17</td>
<td>C</td>
<td>25</td>
</tr>
<tr>
<td>C3</td>
<td>F</td>
<td>44</td>
<td>170</td>
<td>96</td>
<td>T8</td>
<td>35</td>
<td>C</td>
<td>12</td>
</tr>
<tr>
<td>C4</td>
<td>M</td>
<td>35</td>
<td>173</td>
<td>76</td>
<td>T5</td>
<td>1</td>
<td>C</td>
<td>19</td>
</tr>
<tr>
<td>C5</td>
<td>F</td>
<td>33</td>
<td>166</td>
<td>63</td>
<td>C5–T1</td>
<td>&lt;1</td>
<td>C</td>
<td>13</td>
</tr>
<tr>
<td>C6</td>
<td>F</td>
<td>60</td>
<td>173</td>
<td>78</td>
<td>T4</td>
<td>5</td>
<td>C</td>
<td>10</td>
</tr>
<tr>
<td>D1</td>
<td>F</td>
<td>67</td>
<td>172</td>
<td>73</td>
<td>T1–C1</td>
<td>8</td>
<td>D</td>
<td>41</td>
</tr>
<tr>
<td>D2</td>
<td>M</td>
<td>64</td>
<td>168</td>
<td>114</td>
<td>C5–C6</td>
<td>&lt;1</td>
<td>D</td>
<td>50</td>
</tr>
<tr>
<td>D3</td>
<td>F</td>
<td>34</td>
<td>172</td>
<td>60</td>
<td>T7</td>
<td>8</td>
<td>D</td>
<td>31</td>
</tr>
<tr>
<td>D4</td>
<td>M</td>
<td>63</td>
<td>180</td>
<td>83</td>
<td>C3</td>
<td>5</td>
<td>D</td>
<td>44</td>
</tr>
</tbody>
</table>

Mean ± SD — 49 ± 14 172 ± 7 77 ± 17 — — — 26 ± 15

*Participants with AIS levels C and D.

AIS = American Spinal Injury Association Impairment Scale, C = cervical, F = female, L = lumbar, LEMS = Lower Extremity Motor Score, M = male, SD = standard deviation, T = thoracic.

during the course of an intervention with robot-assisted gait training and additional physical therapy. This pretest-posttest trial is used to assess possible effects of this intervention because it is an essential step before setting up a randomized controlled trial [29]. Cardiorespiratory fitness was evaluated using a graded arm crank exercise test performed at baseline and immediately after the training program. To examine the intensity of the training program, we measured $\dot{V}O_2$ and HR during training sessions at the start and end of the training program.

**Training Program**

The training program consisted of 24 training sessions with a Lokomat device, with additional physical therapy sessions completed within 10 to 16 weeks. Training sessions were performed two or three times per week with at least 1 d of rest between two sessions. Each robotic training session lasted 60 min and contained 20 to 40 min walking time. Subjects trained with an individually adapted walking speed, BWS, and robotic support (guidance force [GF]) in such a way that he or she was able to walk comfortably for about 30 min. Training settings were adjusted individually by optimizing BWS, speed, and GF as long as the training settings were tolerated by the subject. The additional physical therapy sessions consisted of usual home-based therapy at a local physical therapy practice or therapy in the rehabilitation center, which focused mainly on walking ability. This additional physical therapy was individually prescribed.

**Arm Crank Exercise Test**

Each subject performed a discontinuous progressive graded exercise test on an Angio arm ergometer (Lode BV; Groningen, the Netherlands) to assess cardiorespiratory function. The exercise tests were carried out by an experienced researcher. Subjects were asked to avoid food, caffeine, and alcohol intake 2 h prior to the exercise tests. Before the exercise test, resting values of $\dot{V}O_2$ and HR were measured during 5 min of seated rest. In recorded test data, there were no signs of hyperventilation or signs for abnormal electrocardiogram (ECG). The exercise protocol consisted of a minimum of three blocks of 3 min of arm pedaling at 60 rpm. The increase in work load was individually set by the researcher such that subjects needed a minimum of three exercise blocks to reach their peak performance. The estimation was based on the exercise performance (HR) of the first exercise block. Rest after each block (1 min) was included to facilitate the measurements for an additional study (recordings of the ECG and impedance cardiogram, see Meijer et al. [30]). Subjects were verbally encouraged to exercise to exhaustion. The exercise test ended when a subject was not able to continue pedaling at 60 rpm because of exhaustion or when the subject indicated that he or she wanted to stop. During the whole exercise test, $\dot{V}O_2$ was continuously monitored with a spirometer (Oxycon Alpha or Oxycon Mobile, Jaeger; Bunnik, the Netherlands). $\dot{V}O_2$ was measured breath-by-breath and averaged over 5 s intervals. Pre- and posttest were executed following the same procedure. Figure 1 depicts an example of the experimental setup of the exercise test.
Robotic Walking Test

The first measurement was performed during one of the early training sessions (session 6, 7, or 8) when subjects had become accustomed to walking in the device. The last measurement was performed during training session 23 or 24. The timing of assessment was predominantly based on practical reasons (e.g., availability of subjects and measuring equipment). During both measurements, \( \dot{V}O_2 \) was measured in the same way as during the arm crank exercise test. HR was monitored by a Polar sport tester (Polar RS400/Polar RS800 and Polar WearLink belt, Polar Electro Inc; Lake Success, New York) with a 5 s recording rate. Prior to the training sessions, resting values of \( \dot{V}O_2 \) and HR were measured during 5 min of rest in a sitting position. Figure 1 depicts the experimental setup. The procedure of both tested training sessions was as follows:

1. Subjects performed a 5 to 10 min warm up to familiarize themselves with the equipment and to warm up their legs.

2. Part 1: Walking at an individually standardized walking condition. During the first part of the training session, individually adapted walking speed, BWS, and GF were kept constant for at least 4 min to obtain steady-state values of \( \dot{V}O_2 \) and HR. During both tested training sessions, the individually standardized walking settings of the robotic support were identical for each subject.

3. Part 2: Exercise intensity of robotic walking. During the last part of the training session, walking speed, BWS, and GF were adjusted in such a way, representative of a regular training session at that moment, to measure the exercise intensity.

Outcome Measures of Cardiorespiratory Fitness

Eight outcome measures were used from the graded arm crank test. Resting \( VO_2 \) and \( O_2 \) pulse were determined as the average over the last 60 s of quiet sitting. Submaximal \( VO_2 \) and \( O_2 \) pulse were determined as the average of the last 30 s of block 2 of the arm crank exercise test. During block 2, subjects exercised at a submaximal intensity with a constant work load. Peak \( VO_2 \) was determined as the average of the last 20 s of the last block of the arm crank exercise test. Furthermore, the lowest
obtained HR during the last minute of seated rest was used as resting HR; submaximal HR was determined as the average of the last 30 s of block 2, and peak HR was the highest HR found in the last block (block 3). The recorded ECG was used to determine the resting, submaximal, and peak HR and resting and submaximal \( \dot{V}O_2 \) pulse. \( \dot{V}O_2 \) pulse as a measure for cardiovascular efficiency was determined according to the following (Equation (1)):

\[
\dot{V}O_2\text{pulse (mL/beat)} = \frac{\text{Oxygen consumption (mL/min)}}{\text{Heart rate (bpm)}}. \tag{1}
\]

A higher submaximal \( \dot{V}O_2 \) pulse after the training program would therefore indicate an improvement in cardiovascular efficiency. Changes in submaximal \( \dot{V}O_2 \) at a given workload would reflect changes in mechanical efficiency (e.g., due to better coordination of arm muscles).

### Outcome Measures of Robotic Walking Intensity

Nine outcome measures from the robotic walking trials were used for analysis. Resting \( \dot{V}O_2\text{robot} \) was determined as the average of the last 60 s during seated rest. Resting HR\(_{\text{robot}}\) was determined as the lowest obtained HR during sitting. Furthermore, the average of values over 10 min of robotic walking during the last part of the training session were determined (\( \dot{V}O_2\text{robot} \) and HR\(_{\text{robot}}\)). Finally, steady-state values of \( \dot{V}O_2 \) and HR, measured during the standardized robotic walking task, were calculated by averaging the last 60 s of walking at the specific standardized walking condition. \( \dot{V}O_2\text{robot} \) measures were expressed as a percentage of \( \dot{V}O_2 \) reserve (%\( \dot{V}O_2\text{R} \)) [31] and metabolic equivalents (METs) [31], and HR\(_{\text{robot}}\) was expressed as a percentage of HR reserve (%HRR) [31]. The %HRR, %\( \dot{V}O_2\text{R} \), and METs were used as measures for the exercise intensity of the training program and were calculated using the following (Equations (2)–(4)):

\[
\%\text{HRR} = \frac{\text{HR}_{\text{robot}} - \text{HR}_{\text{rest}}}{\text{HR}_{\text{peak}} - \text{HR}_{\text{rest}}} \times 100. \tag{2}
\]

\[
\%\dot{V}O_2\text{R} = \frac{\dot{V}O_2\text{robot} - \dot{V}O_2\text{rest}}{\dot{V}O_2\text{peak} - \dot{V}O_2\text{rest}} \times 100. \tag{3}
\]

\[
\text{METs} = \frac{\dot{V}O_2\text{robot}}{\dot{V}O_2\text{rest}}. \tag{4}
\]

Subsequently, the obtained %HRR, %\( \dot{V}O_2\text{R} \), and METs were compared with exercise intensity recommendations for sedentary people [31]. ACSM guidelines for sedentary and/or extremely deconditioned non-disabled adults recommend training at an intensity of 30 to 45%HRR or %\( \dot{V}O_2\text{R} \) in order to maintain or improve physical fitness.

### Statistical Analysis

After checking whether the data followed a normal distribution, paired \( t \)-tests were used to determine whether there were significant differences in resting, submaximal, and peak \( \dot{V}O_2 \), HR, and \( \dot{V}O_2 \) pulse between pre- and posttest arm crank tests or between both tested training sessions. Mean ± standard deviation was computed (but not all reported) for all outcome measures (Tables 2–3). Furthermore, the mean differences (with 95% confidence interval) were also calculated. All statistical analyses were performed using SPSS version 19.0 for Windows (IBM Corporation; Armonk, New York). The significance level was set at 5 percent.

### RESULTS

#### Arm Crank Exercise Test

One subject was unable to perform the arm crank exercise test due to inability to pedal with the device. Figure 2 depicts the individual values of resting HR and \( \dot{V}O_2 \) pulse; submaximal HR, \( \dot{V}O_2 \) pulse, and \( \dot{V}O_2 \); and peak \( \dot{V}O_2 \). Table 2 shows the resting, submaximal, and peak values of \( \dot{V}O_2 \) (absolute and normalized for body mass), HR, and \( \dot{V}O_2 \) pulse measured during both tests. As expected, the \( t \)-test showed no significant difference in submaximal \( \dot{V}O_2 \) between pre- and posttest, but submaximal HR was significantly lower after the training program (Table 2, Figure 2). As a result of a lower submaximal HR at the similar submaximal \( \dot{V}O_2 \), submaximal \( \dot{V}O_2 \) pulse tended to be higher during the posttest. In line with submaximal values, resting HR was significantly lower at posttest than at pretest.

#### Robotic Walking Test

No changes were found in \( \dot{V}O_2\text{robot} \) and HR\(_{\text{robot}}\) between the first and last tested training sessions (Table 3). Although not significant (\( p < 0.1 \)), almost all subjects had lower steady-state \( \dot{V}O_2 \) and HR during the standardized robotic walking task at the last training session compared...
Table 2.
Mean ± standard deviation (SD) of resting, submaximal, and peak oxygen consumption (\(\dot{V}O_2\)), heart rate (HR), and \(O_2\) pulse measured during both arm crank exercise tests (pre- and posttest) \((n = 9)\).

<table>
<thead>
<tr>
<th>Outcome Measure</th>
<th>Pretest (mean ± SD)</th>
<th>Posttest (mean ± SD)</th>
<th>Difference* Mean (95% CI)</th>
<th>t-Value</th>
<th>p-Value</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Resting Value</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(\dot{V}O_2) (mL·min(^{-1}))</td>
<td>247 ± 57</td>
<td>249 ± 61</td>
<td>2 (−29 to 33)</td>
<td>0.15</td>
<td>0.89</td>
</tr>
<tr>
<td>HR (bpm)</td>
<td>77 ± 141</td>
<td>70 ± 12</td>
<td>−8 (−14 to −1)</td>
<td>−2.80</td>
<td>0.02†</td>
</tr>
<tr>
<td>(O_2) pulse (mL·beat(^{-1}))</td>
<td>3.0 ± 0.5</td>
<td>3.4 ± 1.0</td>
<td>0.4 (−0.2 to 0.9)</td>
<td>1.49</td>
<td>0.17</td>
</tr>
<tr>
<td><strong>Submaximal Value</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(\dot{V}O_2) (mL·min(^{-1}))</td>
<td>750 ± 182</td>
<td>741 ± 209</td>
<td>−9 (−75 to 58)</td>
<td>−0.30</td>
<td>0.77</td>
</tr>
<tr>
<td>HR (bpm)</td>
<td>116 ± 14</td>
<td>109 ± 15</td>
<td>−7 (−13 to −2)</td>
<td>−2.95</td>
<td>0.02†</td>
</tr>
<tr>
<td>(O_2) pulse (mL·beat(^{-1}))</td>
<td>6.5 ± 1.7</td>
<td>6.9 ± 2.0</td>
<td>0.4 (−0.3 to 1.1)</td>
<td>1.42</td>
<td>0.19</td>
</tr>
<tr>
<td><strong>Peak Value</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(\dot{V}O_2) (mL·min(^{-1}))</td>
<td>1,163 ± 407</td>
<td>1,207 ± 402</td>
<td>44 (−120 to 208)</td>
<td>0.62</td>
<td>0.55</td>
</tr>
<tr>
<td>(\dot{V}O_2) (mL·min(^{-1}·kg(^{-1}))</td>
<td>15.7 ± 5.1</td>
<td>16.5 ± 5.7</td>
<td>0.8 (−1.4 to 3.0)</td>
<td>0.84</td>
<td>0.43</td>
</tr>
<tr>
<td>HR (bpm)</td>
<td>153 ± 27</td>
<td>152 ± 27</td>
<td>−1 (−7 to 5)</td>
<td>−0.36</td>
<td>0.73</td>
</tr>
</tbody>
</table>

Table 3.
Mean ± standard deviation (SD) values of oxygen consumption (\(\dot{V}O_2\)) and heart rate (HR) together with exercise intensity measures determined during training session at start (first training) and end (last training) of training program.

<table>
<thead>
<tr>
<th>Measure</th>
<th>n</th>
<th>First Training (mean ± SD)</th>
<th>Last Training (mean ± SD)</th>
<th>Difference* Mean (95% CI)</th>
<th>t-Value</th>
<th>p-Value</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Robotic Walking</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>(\dot{V}O_2)robot (mL·min(^{-1}))</td>
<td>10</td>
<td>536 ± 226</td>
<td>492 ± 203</td>
<td>−44 (−109 to 21)</td>
<td>−1.54</td>
<td>0.16</td>
</tr>
<tr>
<td>(\dot{V}O_2)robot (mL·min(^{-1}·kg(^{-1}))</td>
<td>10</td>
<td>6.8 ± 2.2</td>
<td>6.4 ± 2.2</td>
<td>−0.5 (−1.3 to 0.3)</td>
<td>1.30</td>
<td>0.23</td>
</tr>
<tr>
<td>HRrobot (bpm)</td>
<td>10</td>
<td>94 ± 13</td>
<td>88 ± 10</td>
<td>−6 (−13 to 2)</td>
<td>−1.73</td>
<td>0.12</td>
</tr>
<tr>
<td>Steady-state (\dot{V}O_2) (mL·min(^{-1}))</td>
<td>10</td>
<td>558 ± 267</td>
<td>453 ± 184</td>
<td>−105 (−215 to 4)</td>
<td>−2.17</td>
<td>0.06</td>
</tr>
<tr>
<td>Steady-state HR (bpm)</td>
<td>10</td>
<td>94 ± 16</td>
<td>84 ± 9</td>
<td>−10 (−19 to 0)</td>
<td>−2.26</td>
<td>0.05</td>
</tr>
<tr>
<td><strong>Exercise Intensity</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>%(\dot{V}O_2)R</td>
<td>8</td>
<td>23 ± 14</td>
<td>20 ± 13</td>
<td>3 (−9 to 3)</td>
<td>−1.01</td>
<td>0.35</td>
</tr>
<tr>
<td>%HRR</td>
<td>7</td>
<td>23 ± 10</td>
<td>14 ± 11</td>
<td>−8 (−16 to −0.3)</td>
<td>−2.56</td>
<td>0.04†</td>
</tr>
<tr>
<td>MET</td>
<td>10</td>
<td>2.2 ± 0.9</td>
<td>2.1 ± 0.9</td>
<td>−0.1 (−0.4 to 0.1)</td>
<td>−1.37</td>
<td>0.21</td>
</tr>
</tbody>
</table>

*Difference = posttest − pretest.
†Significant difference \((p < 0.05)\) between both tested sessions.

with the first tested training session. Two subjects (D2 and D4) obtained their peak \(\dot{V}O_2\) and HR during robotic walking instead of the arm crank exercise test. Therefore, it was not possible to calculate valid values for %HRR and %\(\dot{V}O_2\)R of robotic walking for these subjects. Also, the %HRR of the last tested training session of subject D1 was excluded from the analyses, because during the whole training session, the HRs of subject D1 were substantially higher than all other tests, resulting in a much higher %HRR. For the remaining individuals, no significant differences in %\(\dot{V}O_2\)R and METs were found between the start and end of the training program (Table 3). However, %HRR was significantly lower at the last training session than the first tested session.

Figure 3 presents individual results of %\(\dot{V}O_2\)R, %HRR, and METs obtained at both tested training sessions. Based on the %\(\dot{V}O_2\)R measured at the first tested training session, only subjects C3, C4, and D1 met the recommended guidelines of exercise intensity. During the last training session, subjects C3, D1, and D3 achieved
Figure 2.
Individual values of (a) resting heart rate (HR), (b) resting O₂ pulse, (c) submaximal HR, (d) submaximal O₂ pulse, (e) submaximal oxygen consumption (VO₂), and (f) peak VO₂ measured during both arm crank exercise tests (pre- and posttest). Line of identity (y = x), which illustrates no change between pre- and posttest, is also shown in graphs. Resting and submaximal HR at posttest were significantly lower than at pretest. No significant changes were found in resting O₂ pulse, submaximal O₂ pulse, submaximal VO₂, and peak VO₂. AIS = American Spinal Injury Association Impairment Scale, C = participant with AIS level C, D = participant with AIS level D.

a %VO₂R above the minimum recommended value of 30%VO₂R. In the same way, it is illustrated that at the start of the training program, the %HRR of subjects C3, C6, and D1 was above the recommended guidelines. At the end of the training program, only subject C3 exercised at an intensity above 30%HRR. VO₂ during robotic walking was one to three times higher than VO₂ at rest in most subjects. Only subjects C3 and D4 achieved a MET value above 3.0, which is considered exercising at moderate intensity. VO₂ during robotic walking of subject C5 was nearly the same as her resting VO₂.

DISCUSSION

In this study, exercise intensity of walking in the Lokomat was investigated in subjects with iSCI. Results indicated that the exercise intensity in these subjects was predominantly below recommended levels for sedentary persons on both assessments during the study. Based on the submaximal VO₂ and HR values during the arm crank test, this study shows that cardiorespiratory fitness might have increased during the intervention. The fact that there was no change in peak VO₂ of the arm exercise test does...
Individual values of (a) percentage of oxygen consumption reserve (%$\dot{V}O_2R$), (b) percentage of heart rate reserve (%HRR), and (c) metabolic equivalents (METs) of robotic walking during both tested training sessions. Black lines indicate recommended exercise intensity according to American College of Sports Medicine (ACSM) guidelines [31]. Most subjects exercised below this minimum level of exercise intensity.

not necessarily suggest that cardiorespiratory fitness did not improve after the training program. Peak $\dot{V}O_2$ determined during an arm exercise test is mainly limited by local factors (small muscle mass) rather than central factors (lungs or heart) [32–34]. Since the intervention was aimed at the legs, the exercise capacity of the arm muscle was assumed to be unchanged. Because of peripheral limitations, it is conceivable that the peak $\dot{V}O_2$ as measured during an arm crank test did not change, while a subject’s actual aerobic fitness did improve. By considering this limitation, we valued the submaximal values as more informative of whether cardiorespiratory fitness had improved. We used the arm crank test instead of a test using the lower limbs because we wanted to rule out the effect of possible improvements in neurological impairments in the legs elicited by the intervention. Such improvements would have the effect of increased muscle mass being employed during the exercise test, which could lead to a higher $\dot{V}O_2$ that was not due to improvements in cardiorespiratory fitness. It appeared that after the robot-assisted gait training, subjects had a significantly lower submaximal HR during arm crank exercise at the same work load and $\dot{V}O_2$. Although this suggests improved cardiovascular efficiency, we did not find a significantly lower $O_2$ pulse, suggesting that the improvements are rather small. Furthermore, subjects had a significantly lower resting HR after a period of robot-assisted gait training, again suggesting improved cardiorespiratory fitness. Although these results should be interpreted with caution, together these results indicate small improvements in cardiorespiratory fitness.

The small improvements in cardiorespiratory fitness is rather surprising in light of the exercise intensity of the training program. The ACSM guidelines for exercise prescription [31] and Ginis et al. [35] recommend that people with SCI should participate in an aerobic exercise activity of moderate to vigorous exercise intensity (30–60%HRR, 30–60%$\dot{V}O_2R$, or 3.0–6.0 METs) at least twice per week. The majority of the subjects, however, did not reach this minimum level and exercised at very low intensity (<20%$\dot{V}O_2R$ or <20%HRR). In line with findings of the present study, van den Berg et al. found that a low-intensity training program (30%HRR) can improve physical capacity in untrained, nondisabled subjects [36]. Especially for sedentary people, low exercise intensity seems to be safer and is associated with a higher motivation [37]. In this light, robotic walking may be an attractive low-intensity exercise mode for people with iSCI.
Furthermore, the results showed that almost all subjects achieved lower submaximal VO₂ and HR by performing the same robotic walking task after the training period, suggesting an improved ability to employ the assistance of the device or an improvement in “robotic walking economy” [38]. This improved ability to employ the assistance of the device or improvement in robotic walking economy might explain that most subjects had a lower %HRR at the end of the training program than at the start. Furthermore, the average value of %VO₂R was lower at the last training session, suggesting that subjects adapted to the training program. Although during every training session subjects were encouraged to contribute actively to the robotic walking activity, it was not always possible to reduce the robotic support in a way desirable because of spasticity, risk of wounds, and/or muscle weakness. This improved ability to employ the assistance of the device or improved walking economy was also observed in a study of the longitudinal changes in cardiopulmonary function during an intervention with robot-assisted gait training in two subjects with iSCI [38]. Nevertheless, contrary to our results, cardiorespiratory fitness did not improve in that study. Jack et al. suggested that the improvement in robotic walking economy was mainly the result of a better gait pattern instead of changes in cardiopulmonary system [38].

The average level of exercise intensity of robotic walking found in this study (2.2 METs) was higher than found for passive walking in Jack et al. (1.4 METs) [24] but lower than for active walking in studies of Israel et al. [23] and Hunt et al. [39] (2.5 and 4.0 METs, respectively). Israel et al. [23], Hunt et al. [39], and Jack et al. [40] also presented values for peak VO₂ (14, 16, and 28 mL/kg/min, respectively) obtained during maximal active robotic walking that were substantially higher than values of the present study (VO₂robot = 6.8 mL/kg/min). During active walking in these studies, subjects were supposed to push against the orthoses with their legs while walking. When walking with less GF applied to the legs, such instruction would probably lead to emergency stops of the device since safety limits will be surpassed. Another explanation for the difference in exercise intensity between our study and the literature is the level of impairment, given that the legs can be loaded more when less impaired. Relatively more individuals with AIS level D participated in the studies by Israel et al. [23], Hunt et al. [39], and Jack et al. [40] than in our study. It is likely that the greater impairment of subjects in the present study has at least in part contributed to the lower exercise intensities found. Nevertheless, when subjects are encouraged to push against the orthoses of the Lokomat device during walking, as was done in Jack et al. [40], it seems conceivable that exercise intensity can increase.

Limitations of this study are the small sample size and heterogeneity of the study population, the latter resulting in interindividual differences in the level of physical capacity and the differences of exercise intensity of the intervention. Furthermore, the %VO₂R and %HRR were calculated using the resting and peak values of VO₂ and HR. Resting VO₂ was determined after 5 min of quiet sitting, which although commonly used, might not be optimal when assessing resting values [41]. This might have resulted in overestimation of the resting values of VO₂ and HR, which in turn, results in underestimation of %VO₂R and %HRR. On the other hand, the possibility exists that peak values of VO₂ and HR were underestimated because of different factors such as subject motivation, day-to-day variations, the exercise protocol, and exercise modality. For this reason, the %HRR of the last assessment of subject D1 was excluded from the analyses. Furthermore, it was not possible to calculate valid values of %VO₂R and %HRR in two subjects (D2 and D4), because they obtained their peak VO₂ and HR during robotic walking instead of during the arm crank exercise test. An alternative would be that peak HR would be estimated based on age. However, this could result in overestimation of the maximal HR since individuals with SCI above thoracic level 4 may have impaired sympathetic innervations of the heart. Therefore, we chose the method presented in this article. To complement the results of the %VO₂R and %HRR, we also calculated MET values. By comparing the VO₂ and HR of both standardized robotic walking tasks, the assumption was made that external load was kept the same in both conditions. However, in this study, the amount of handrail support, which can influence the external load, was not completely standardized during both tests. Ideally, handrail support should be avoided during the testing period. However, some subjects were not able to walk without handrail support. Despite this possible variation in external load, almost all subjects had a lower VO₂ and HR at the last measurement compared with the first, which still indicates an improvement in robotic walking economy.
CONCLUSIONS

The majority of the subjects exercised below the minimum level of the recommended exercise intensity (<30%\(\dot{V}O_2\)R, <30%HRR, and <3.0 METs). In spite of the low exercise intensity of the training program and no changes in peak \(\dot{V}O_2\) of the arm exercise test, the lower resting and submaximal HR suggest that a period of robot-assisted gait training may have induced some improvement in cardiorespiratory fitness. Furthermore, almost all subjects had lower \(\dot{V}O_2\) and HR during the same robotic walking task after the training period, reflecting a higher robotic walking economy. Therefore, treadmill walking, including robot-assisted walking, might not only help in improving walking ability but also have secondary effects such as improvement in cardiorespiratory fitness, as found in this study. Whether these effects are different from conventional therapy approaches may be studied in future randomized clinical trials.

ACKNOWLEDGMENTS

Author Contributions:
Study concept and design: F. Hoekstra, M. P. M. van Nunen, K. H. L. Gerrits, T. W. J. Janssen.
Acquisition of data: F. Hoekstra, M. H. P. Crins.
Drafting of manuscript: F. Hoekstra.
Statistical analysis: F. Hoekstra.
Obtained funding: K. H. L. Gerrits, T. W. J. Janssen.
Administrative, technical, or material support: F. Hoekstra, M. P. M. van Nunen.
Study supervision: M. P. M. van Nunen, K. H. L. Gerrits, T. W. J. Janssen.

Financial Disclosures: The authors have declared that no competing interests exist.

Funding/Support: This material was based on work supported by the Dutch Heart Foundation (Hartstichting, grant 07.21) and Revalidatiefonds (project 2007166). The study was conducted at Reade Amsterdam Rehabilitation Research Center, Amsterdam, the Netherlands.

Additional Contributions: We thank Thijs Schoots for the assistance with data acquisition. Dr. Stolwijk-Swüste is now with the Department of Rehabilitation, Meander Medical Center, Amersfoort, the Netherlands.

Institutional Review: The study protocol was approved by the ethics committee of the VU University Medical Center Amsterdam. All participants provided written informed consent before enrolling in the study.

Participant Follow-Up: The participants will be informed of the publication of this study.

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http://dx.doi.org/10.1016/j.jada.2006.02.009

Submitted for publication October 17, 2012. Accepted in revised form May 30, 2013.

This article and any supplementary material should be cited as follows: